

# Adaptive Bio-kinematic Control for Secure Rehabilitation Robotic Devices

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# Outlines:

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## State of the art

- Rehabilitation exoskeleton and interest of research
- Existing control strategies and problems
- Co-contraction

## Contributions

- Methods
- Neuro-motor index
- Canonical analysis

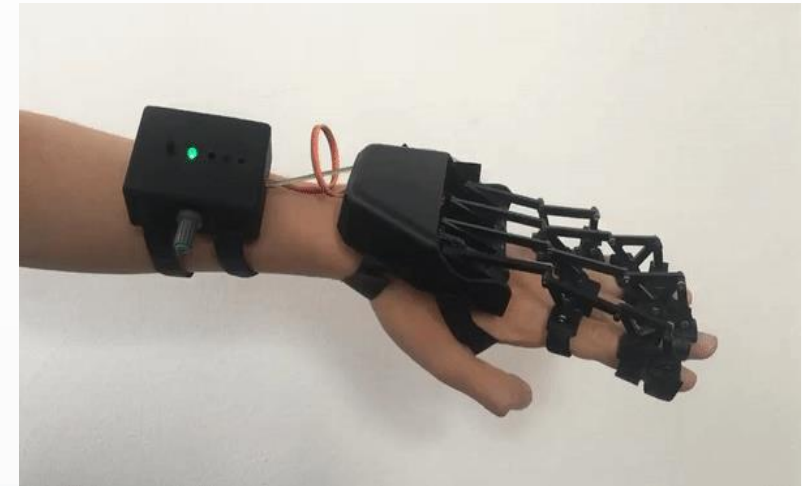
## Results

- Online study ( High level control loop)

## Conclusion

# Rehabilitation Exoskeleton- Assisted Therapy

- Mechatronic device help with several types of movement disorders.
- Increase physical performance.
- Fitted to the shape and function of the human body.



# Rehabilitation Exoskeleton- Lower Limb Therapy



Spastic gait



Scissor gait



Propulsive gait



Steppage gait



Waddling gait

Gait disorder types



Autonomous



Treadmill

Lower limb rehabilitation exoskeleton models



Overground



Active orthoses



Foot-plates

# Control Strategies : Existing Controllers and Problems



Ekso GT

1

Interaction force controllers  
using impedance or admittance

- Predetermined trajectories.
- No dynamical adaptation.

## Existing controllers

## Problems

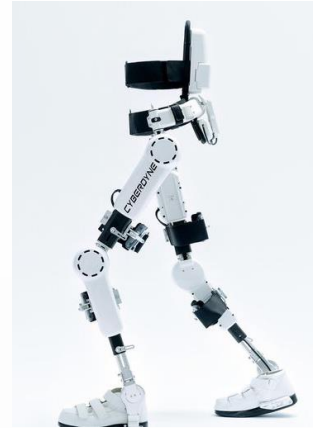
**For both approaches:**

- No assessment of patient possibilities
- Inadequate for specific patient's walk.

2

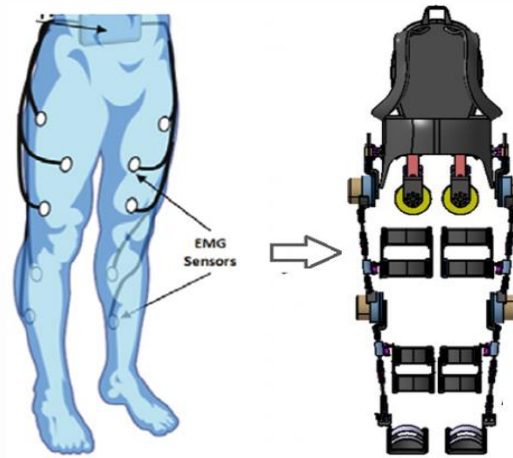
Musculoskeletal model  
based on EMG signals

- EMG signals variability
- Walking speed induces non-linear variations
- Inapplicable when muscle disorder.



HAL

# Control Strategies : Needs and Goal



SOL exoskeleton - IISV

## Inter-active Controller

### Needs

- Assistance as needed.
- Patient expertise.
- Intention Detection.

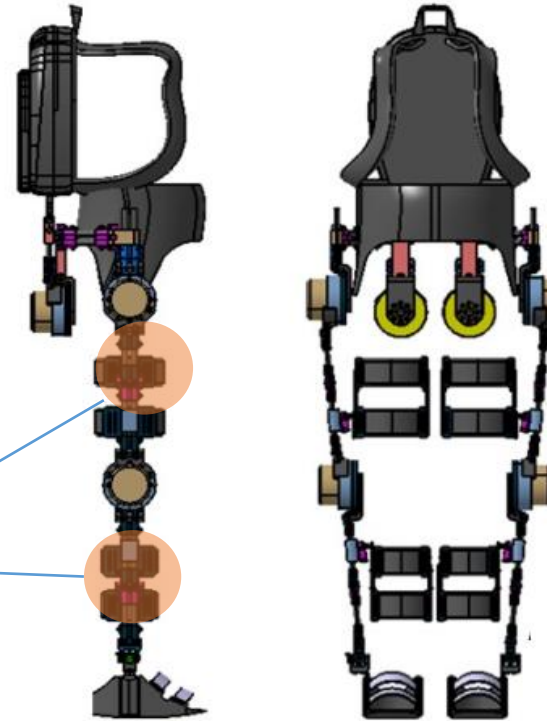
### Goal

- Modularity.
- Stability.
- Security.

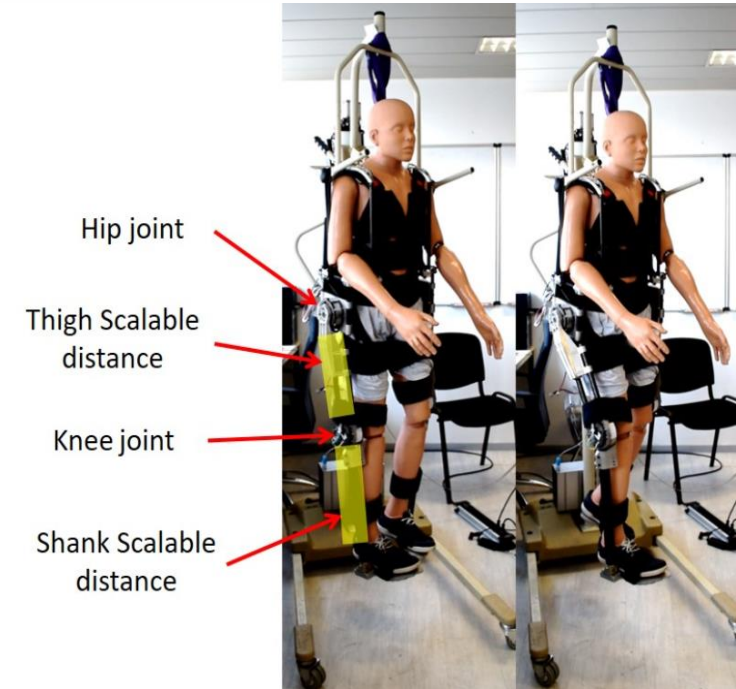
# Sol Scalable Exoskeleton Designed by Samer ALFAYD Team's

- Active actuators: in the hip and knee
- Scalable with age
- **Control strategy tested now :**  
Compatible with walking problems that result from the central nervous system (CNS) spinal cord injury, Cerebral palsy, and Stroke

Active actuators

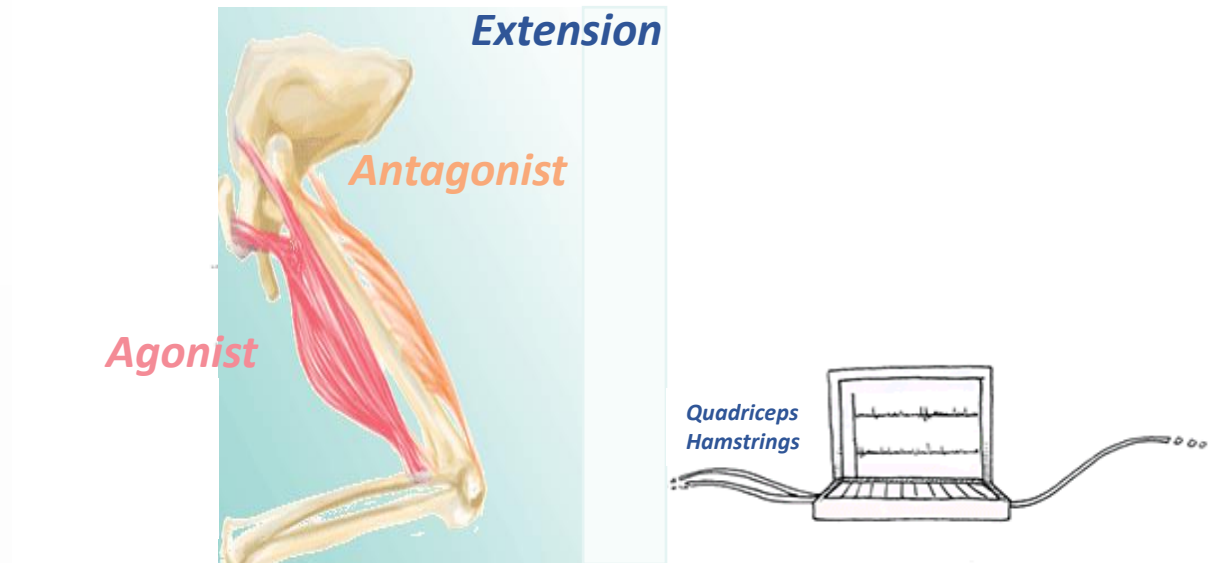


SOL Scalable exoskeleton



M. Kardofaki, N. Tabti, S. Alfayad, , F. B. Ouezdou, Y. Chitour, and E. Dychus, "Mechanical development of a scalable structure for adolescent exoskeletons," in 2019 IEEE, ICRA

# Co-contraction : Co –Contraction Index, Why ?



➤ Related to joint stability

*(Basmajian 1977 )*

➤ Indicates the achievement of a motor skill

*(Best 2017 )*

➤ Important factor which contributes to the inefficiency of pathological movement

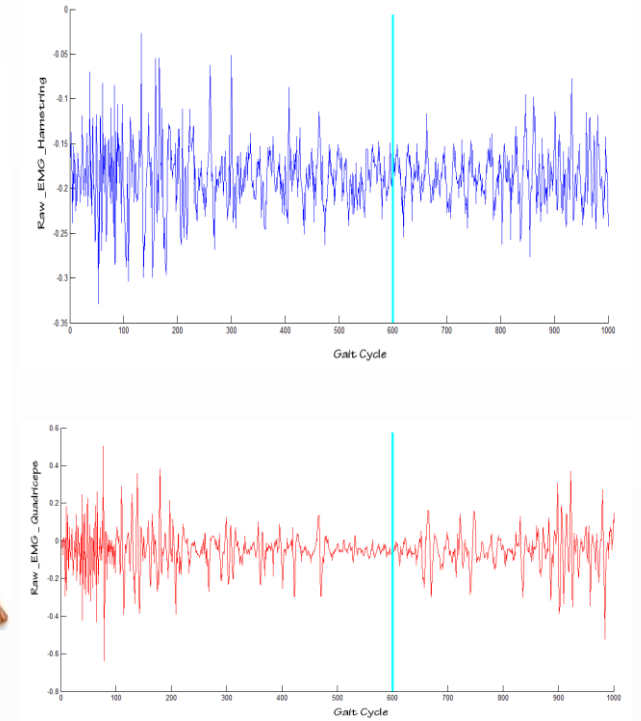
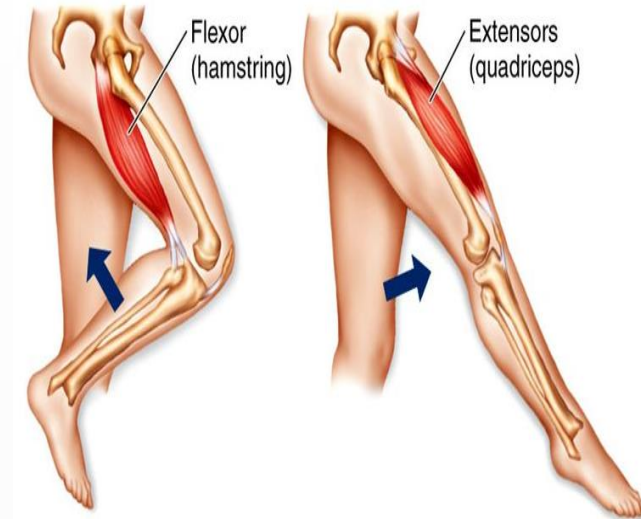
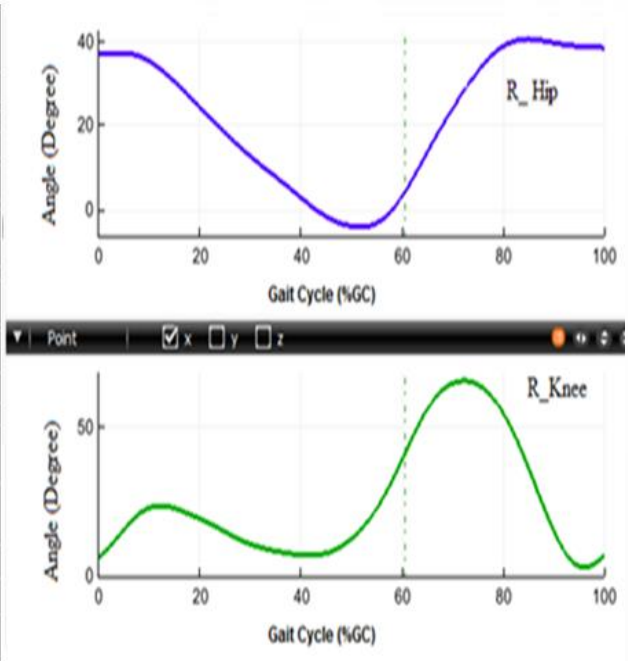
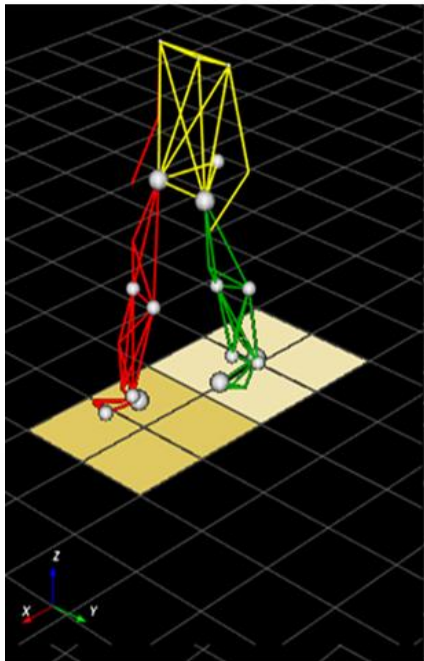
*(Winter 1985)*

➤ Based on EMG , These signals contain information about the intention of the patient

*(Lenzi 2012 )*



# Methods: Bio-kinematic Data



placement of electrodes for kinematic data using MOKKA.

Representation of kinematic data using MOKKA.

Bi-articular muscle group for hip and knee movement.

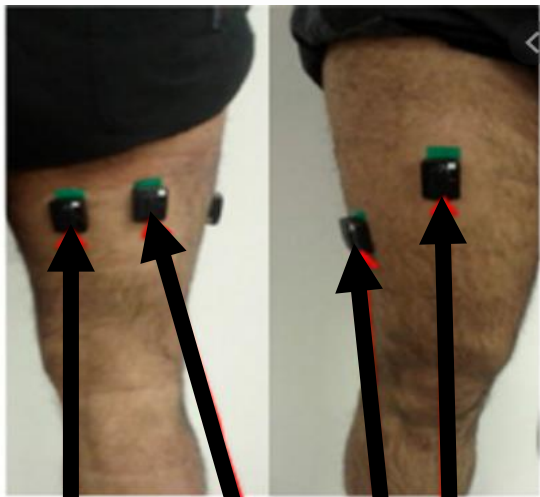
Raw EMG for Hamstrings and Quadriceps using MATLAB.

# Methods: Bio- kinematic Processing

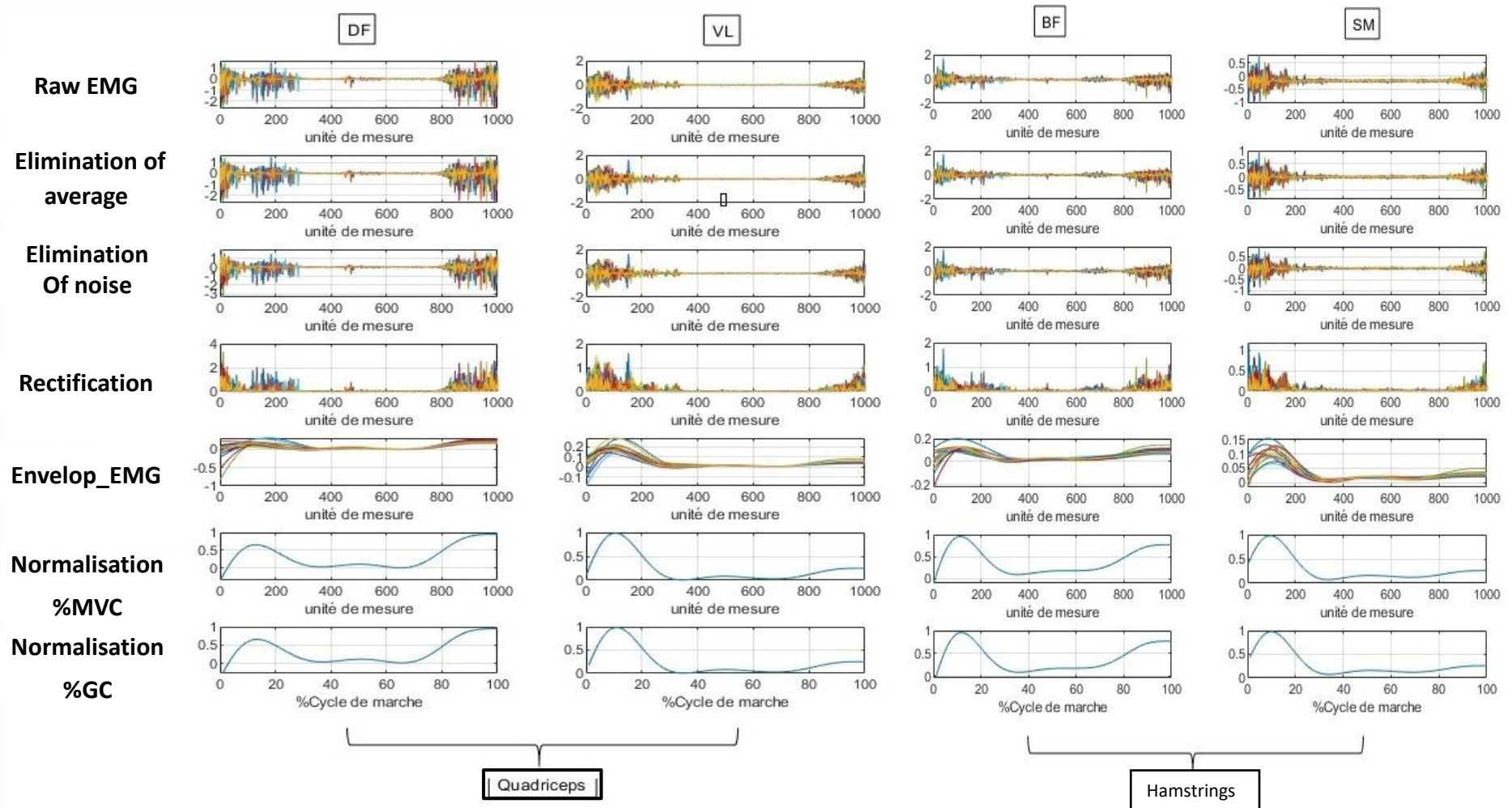
## EMG Processing

**20 Subjects healthy, CP, Stroke**

- 11 GC to 1000 points
- Frequency % patient cadence
- Normalisation % MVC and GC



Semi Membranous Femoris    Biceps Femoris Lateral    vastus Rectus Femoris



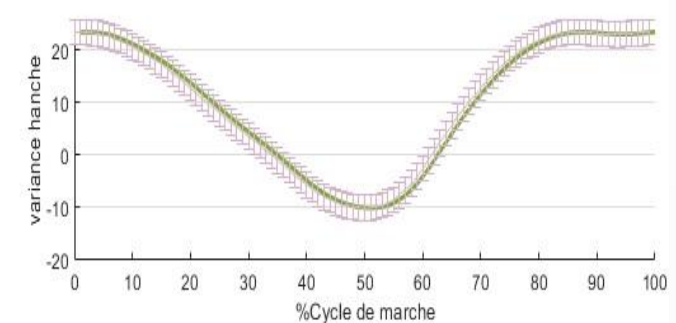
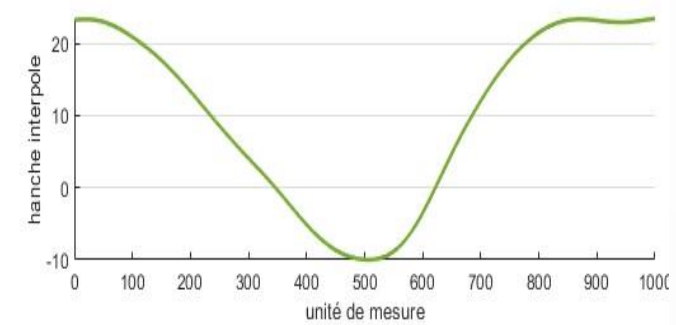
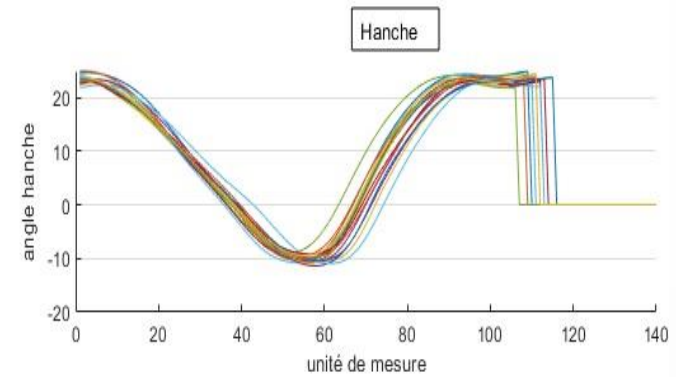
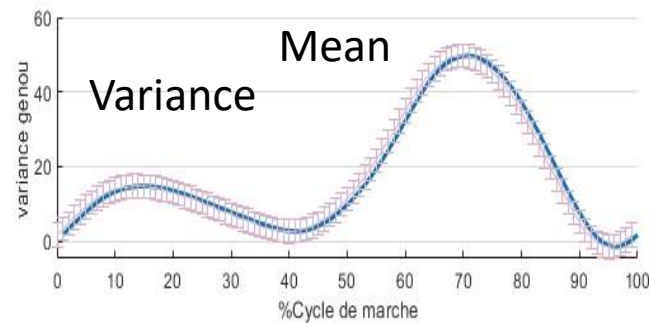
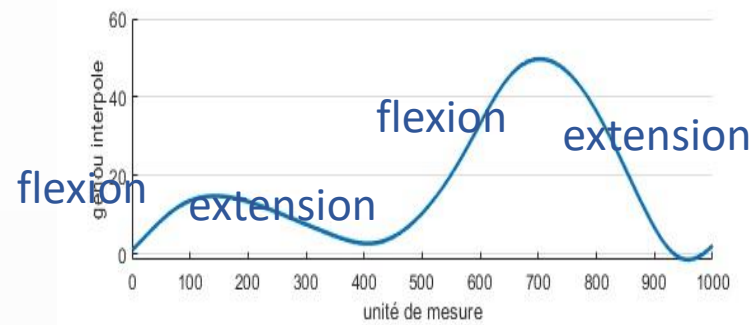
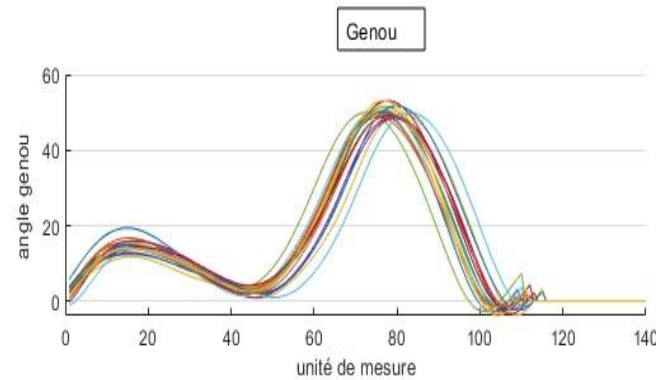
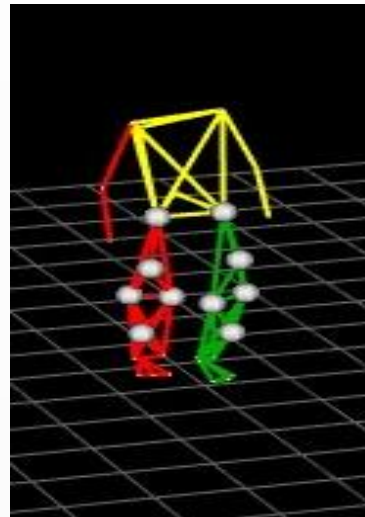
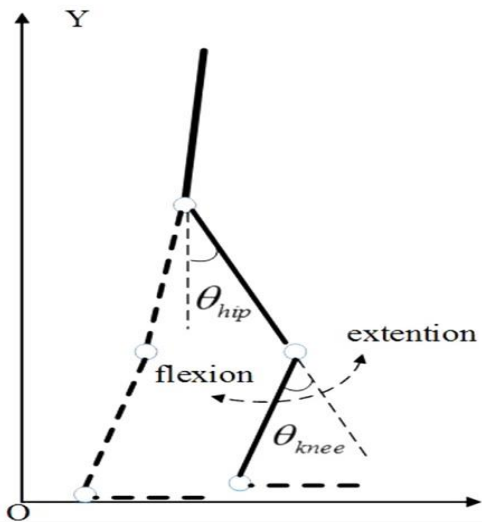
Shiavi et.al .1998  
Hesse et al. 2000

# Methods: Bio-kinematic Processing

## Angular Kinematic :

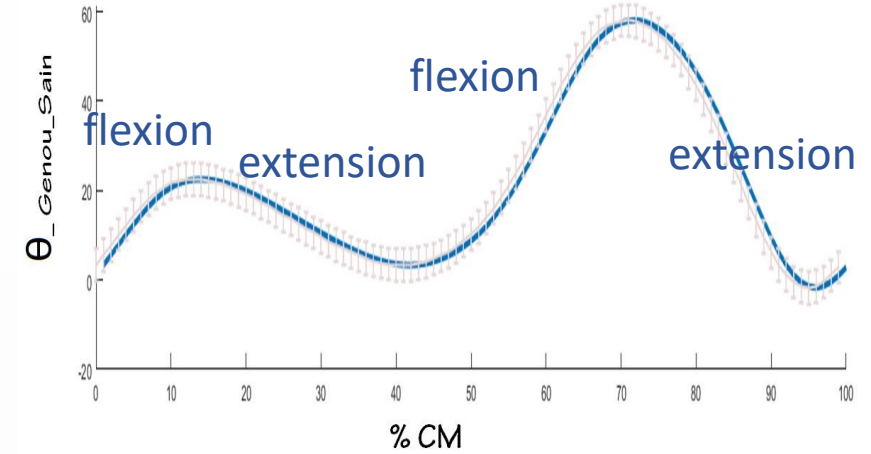
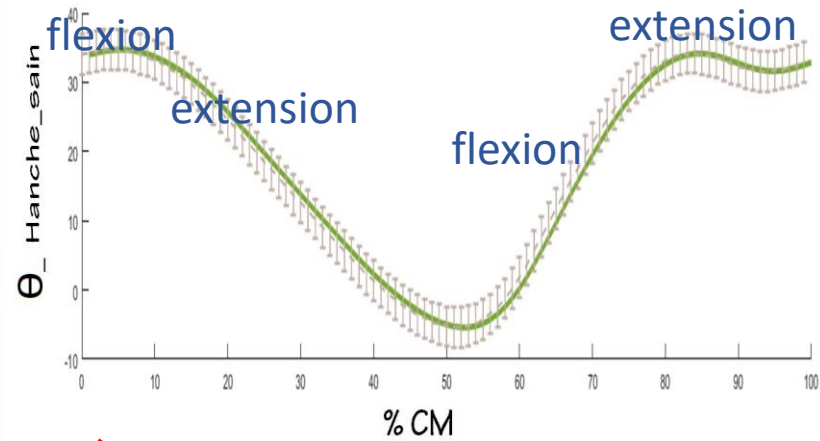
### 20 Subjects healthy, CP, Stroke

- 11 gait cycles (GC)
- Interpolation at 1000 points
- Mean and variance
- Indication of disorder (flexion/extension)

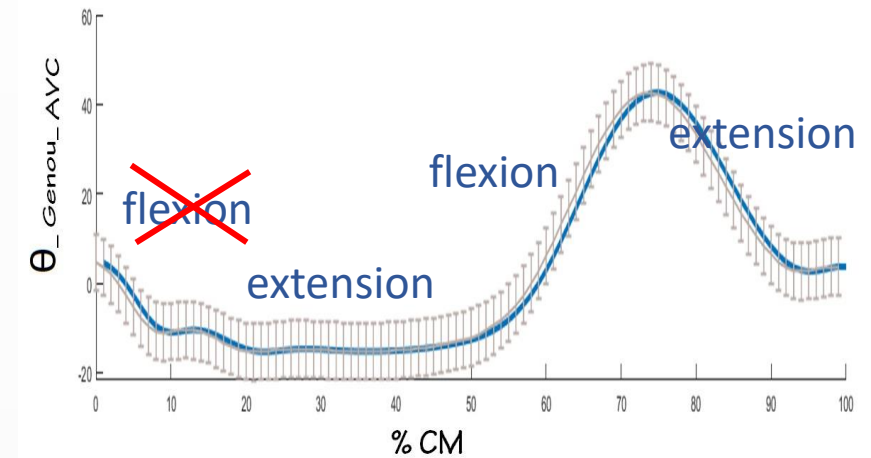
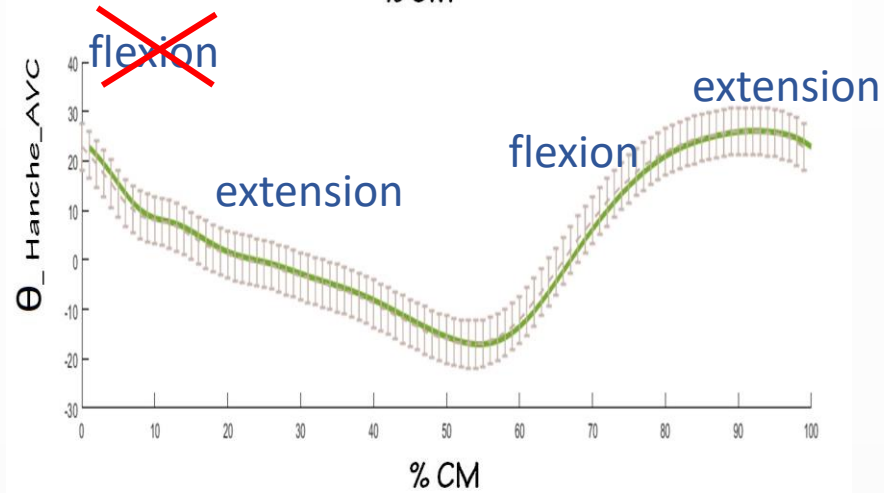


# Methods: Bio-kinematic Processing

Joint Angles  
Healthy subject



Joint Angles  
CP subject



# Neuro – Motor : Proposed Index

$$f(t) = ENV(emg_{ATNAGO}(t) \cap emg_{AGO}(t))$$

Detection of peaks  $f(t) : \operatorname{argmin}_t | f'(t) |$

$$\triangleright R_x(t) = h_1(t) \cdot f_0 + h_2(t) \cdot p_0 + h_3(t) \cdot f_1 + h_4(t) \cdot p_1$$

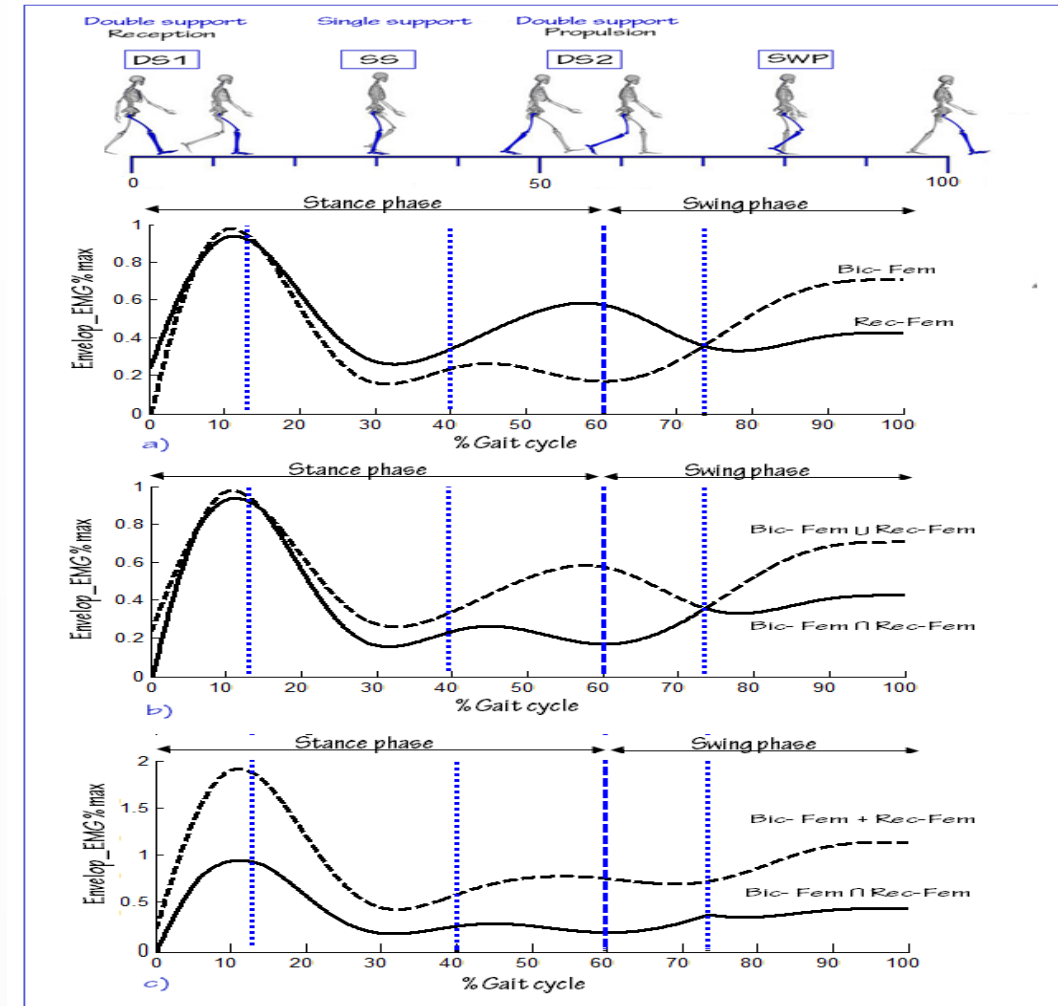
$\triangleright$  when  $h_1, h_2, h_3$  et  $h_4 \in He$ ;  $p_0$  et  $p_1$  tangent à  $f_0$  et  $f_1$

$$INM = A(t) \left[ \frac{1}{B(t)} + \frac{R_x(t)}{C(t)} \right]$$

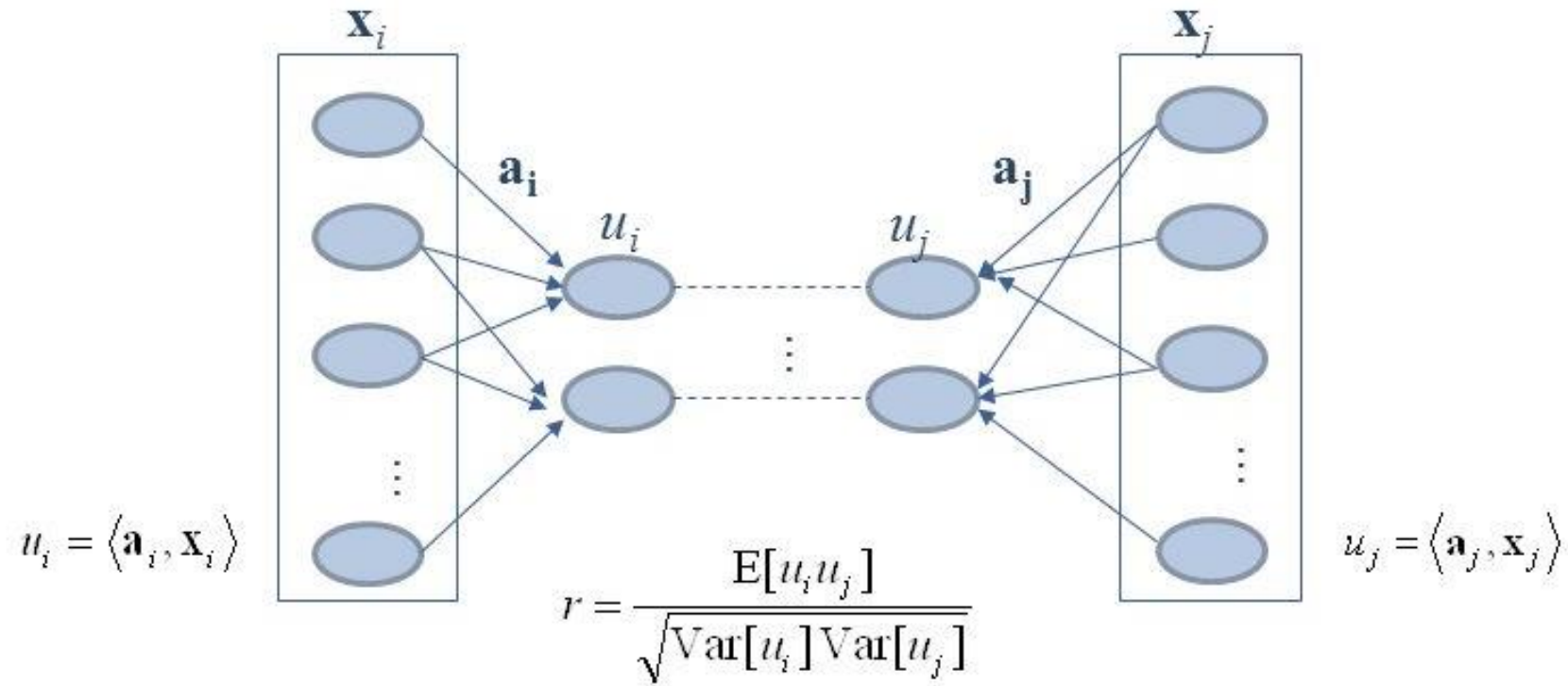
$$A(t) = \int_{t1}^{t2} (ENV_{emg-ago}(t) \cap ENV_{emg-anta}(t) dt)$$

$$B(t) = \int_{t1}^{t2} (ENV_{emg-ago}(t) \cup ENV_{emg-anta}(t) dt).$$

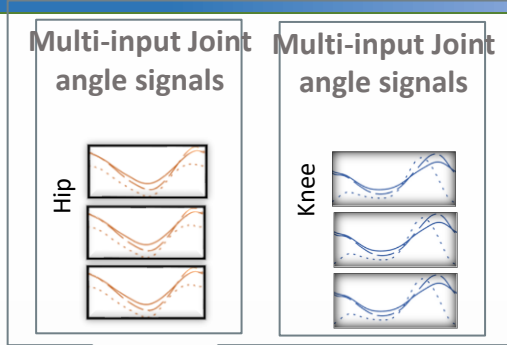
$$C(t) = \int_{t1}^{t2} (ENV_{emg-ago}(t) + ENV_{emg-anta}(t) dt).$$



# Canonical Correlation Analysis : what is it?

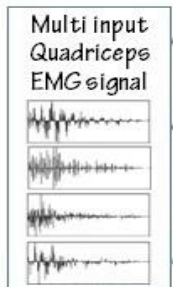
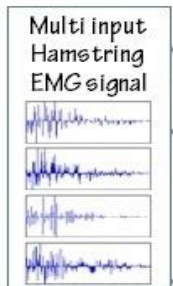


# Online Study : Precision of Command Angle



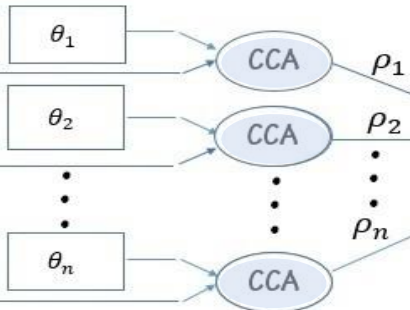
$\Theta_{ref}$  = joint angle data from a healthy subject (compatible with the patient (speed, weight, and body length, as possible))

$\Theta_P$

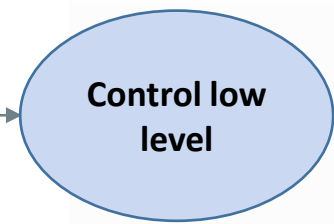
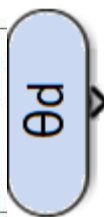


$I_1$   
 $I_2$   
 $\vdots$   
 $I_n$   
 $I$

$\theta_{ref}$   
Reference joint\_angles



$\Theta_d(t)$



Input

Applied method

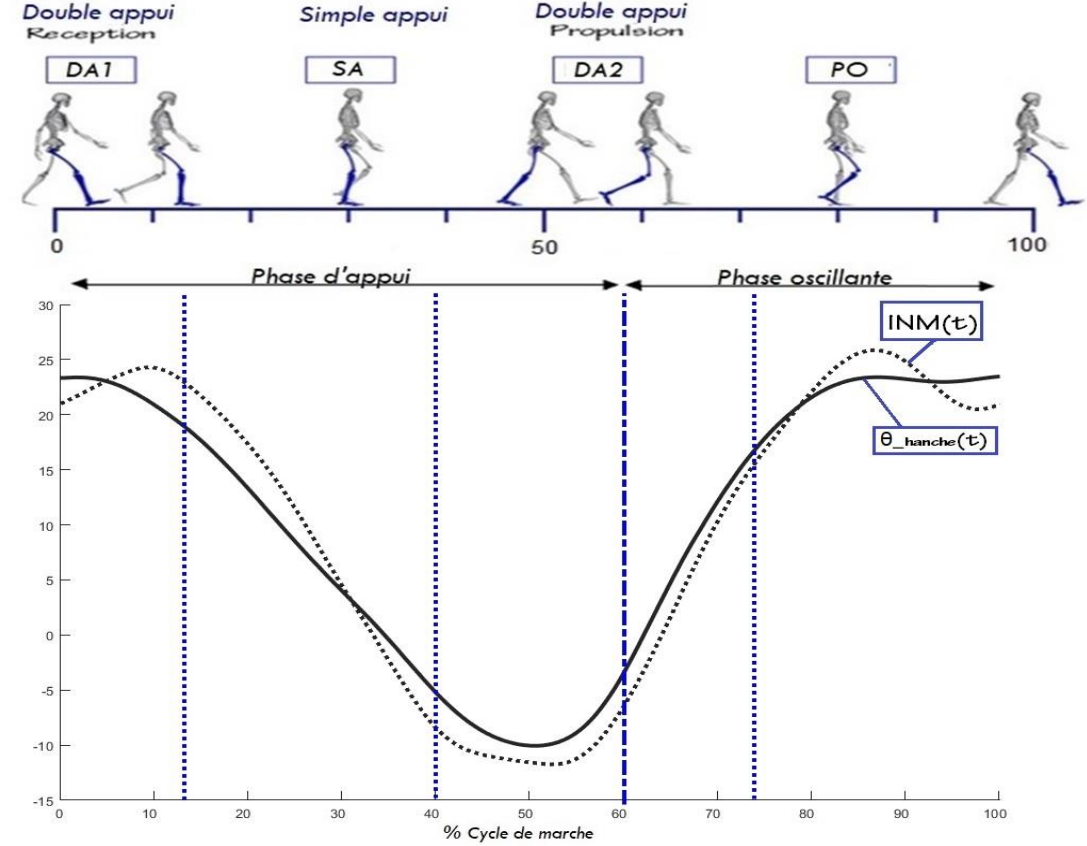
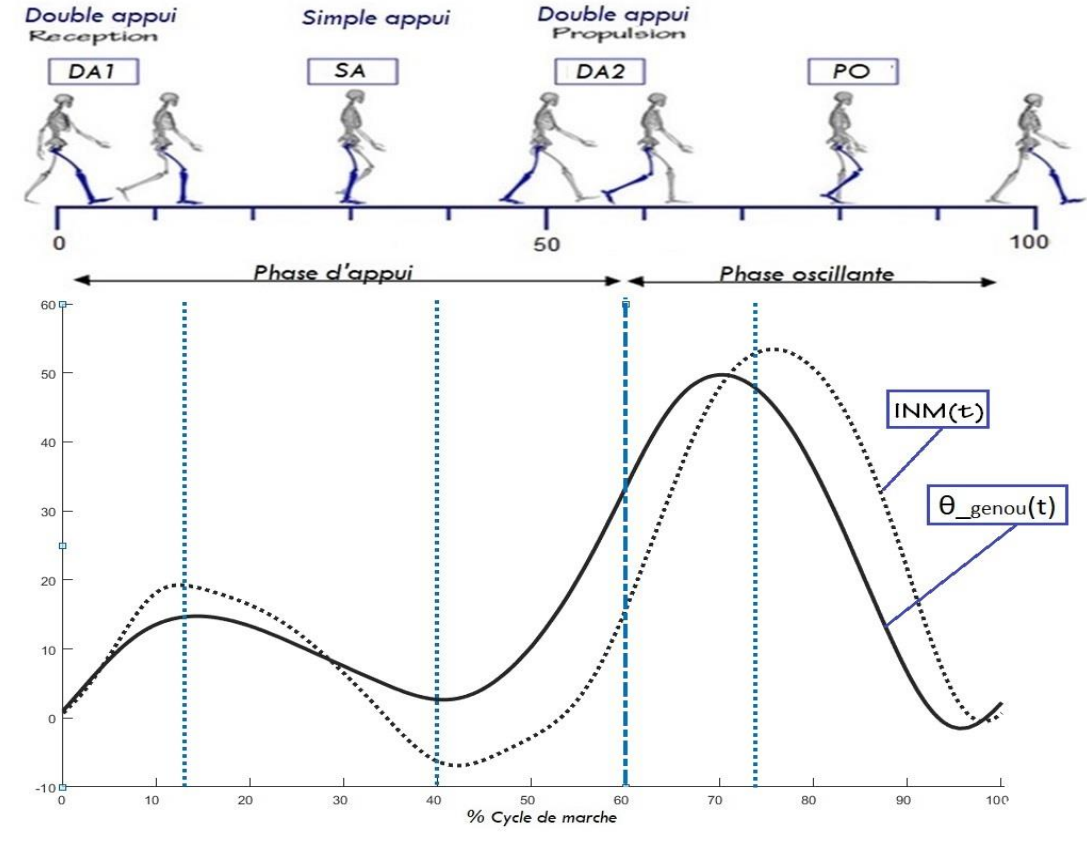
output

$$\max_{(W_I, W_\Theta)} \rho(I, \Theta) = \frac{E(I^T \Theta)}{\sqrt{E(I^T I)E(\Theta^T \Theta)}}$$

$$= \frac{E(W_I^T I I^T W_\Theta)}{\sqrt{E(W_I^T I I^T W_I) E(W_\Theta^T \Theta \Theta^T W_\Theta)}}$$

- 1- Input signals (+ Processing)
- 2- Determine  $\theta = f(I, N, M)$
- 3- Select  $\theta_d = CCA(\theta, \theta_{ref})$

# Healthy subject : Estimation of joint angle from NMI

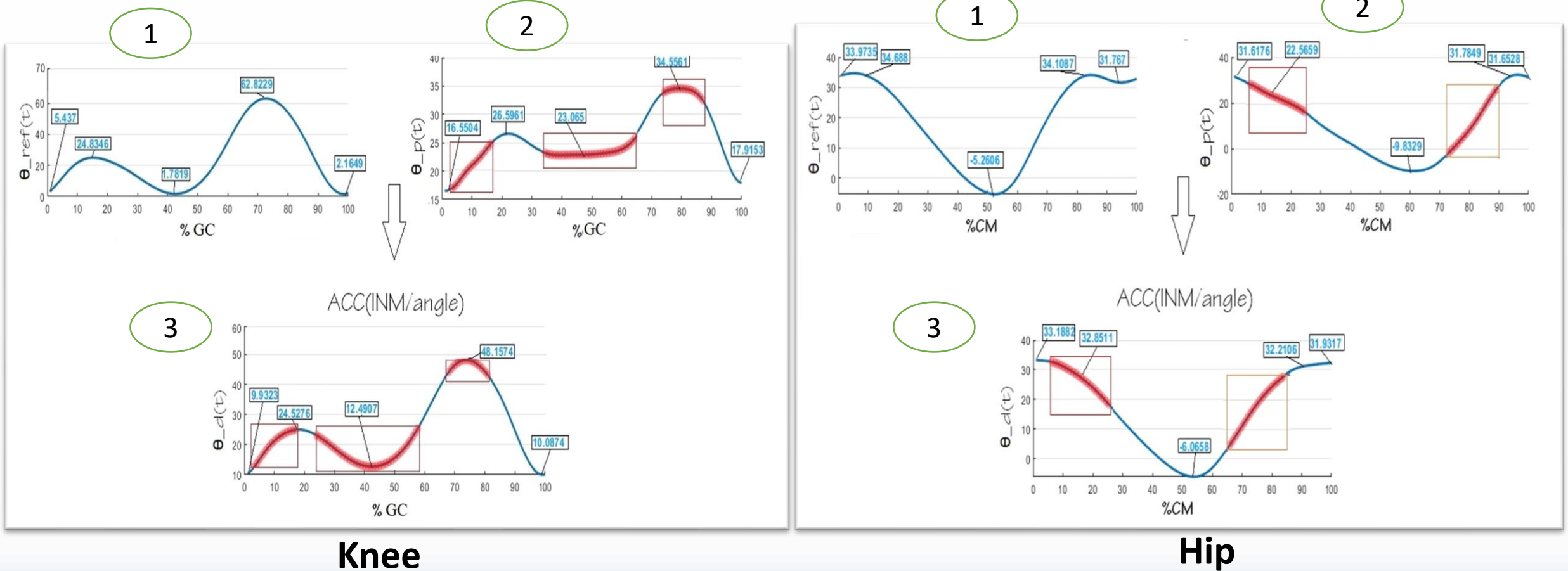




# Results

Finally, the correction of the kinematic curves for 11 neurological patients (with CP and Stroke) is testing:

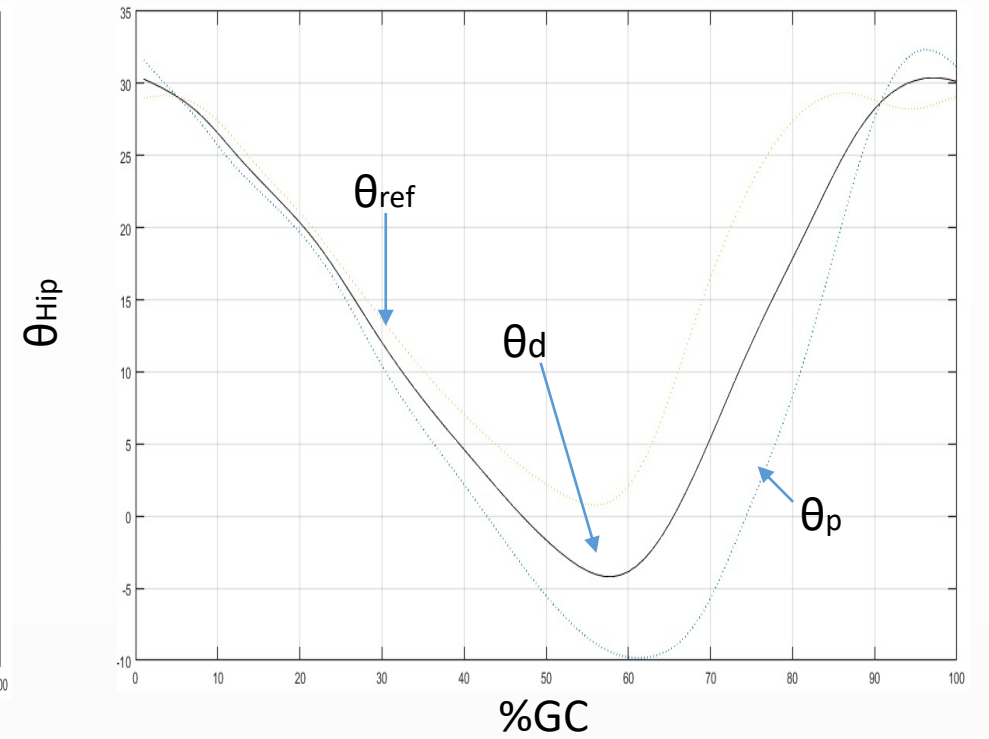
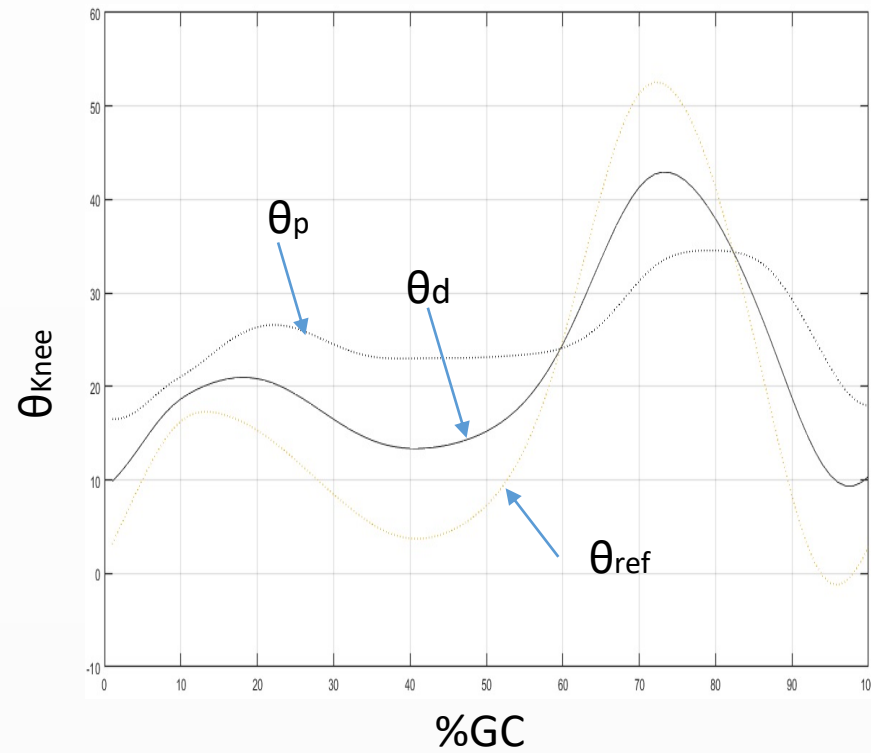
The rate was achieved reaches 45% to 82%



# Results

## Characteristics of $\Theta_d$ :

- Have values between  $\theta_p$  and  $\theta_{ref}$
- Respect the expertise of the patient and his muscle capacity



# Conclusion and Perspective

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- **Control an exoskeleton is important but it should be done with collaboration.**
- **The effectiveness of using (NMI) for bio kinematic-based control strategy for user-lead rehabilitation exoskeleton was investigated to achieve the needed collaboration in respect to the capacity of muscle patient.**
- **The CCA method is used for extracting the better angle information ( $\theta_d$ ) from the multi EMG signals .**
- **$\theta_d$  is the output of our high-level loop and will be the input for the low-level loop using PID controller for SOL Exoskeleton**

***Thank you***